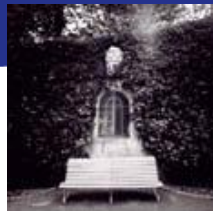




**BC Cancer Agency**

CARE + RESEARCH

*An agency of the Provincial Health Services Authority*



# Modern clinical applications of Monte Carlo simulations for in-vivo patient-specific QA

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Adjunct Professor, University of British Columbia  
Vancouver, Canada***

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*MCMA, Naples, Italy, 17 October 2017*

A truly 'patient-specific' QA protocol should be relevant to the actual patient treatment and be capable of providing *in vivo* dosimetry.

The major current commercially-available QA solutions (e.g. ArcCHECK, MapCheck, EPIdose (Sun Nuclear, USA); Delta4 (ScandiDos, Sweden); or MatriXX (IBA Dosimetry, Germany)), are valuable within the pre-treatment paradigm, but would not be able to catch an egregious error during treatment, such as patient miss-positioning, missing MLC, etc

In contrast, *transmission* EPID dosimetry and patient 3D dose calculation using real-time linac log information, in conjunction with CBCT imaging to assess changes in patient anatomy, could provide adaptive patient dose accumulation over the entire course of treatment

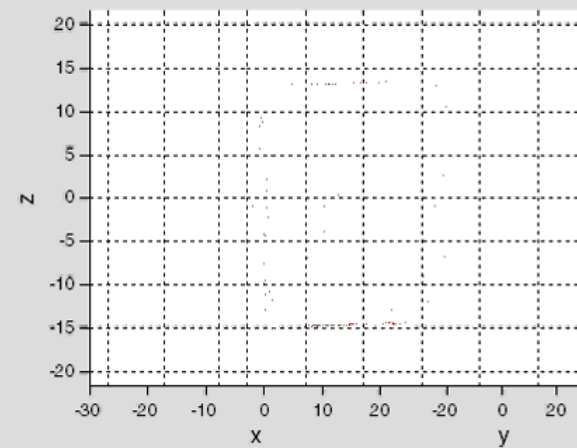
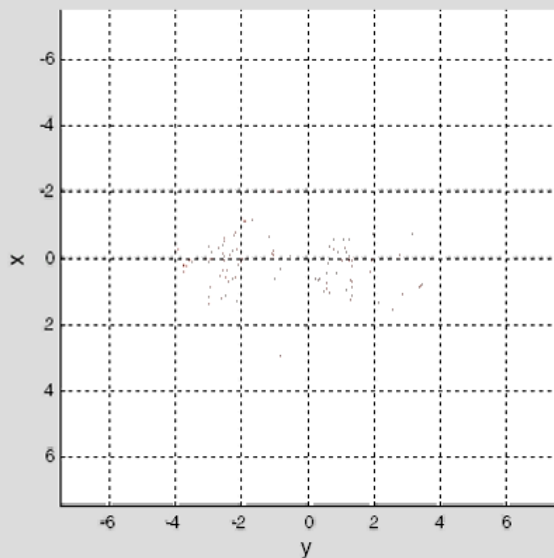
After scoring an output 4D phase space in DOSXYZnrc, the EPID MC dose can be obtained in a single simulation. Since the MU index is stored for each particle, specific control-point information can also be extracted.

Example: VMAT plan with jaw tracking

**MU index:**

● 0.0 ~ 0.5

● 0.5 ~ 1.0

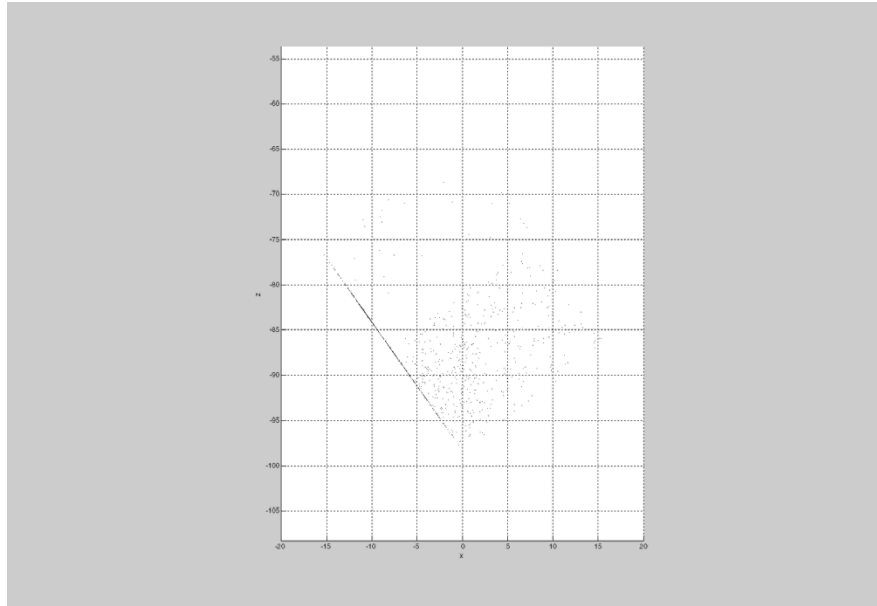


‘Entrance detector’ 4D phase space

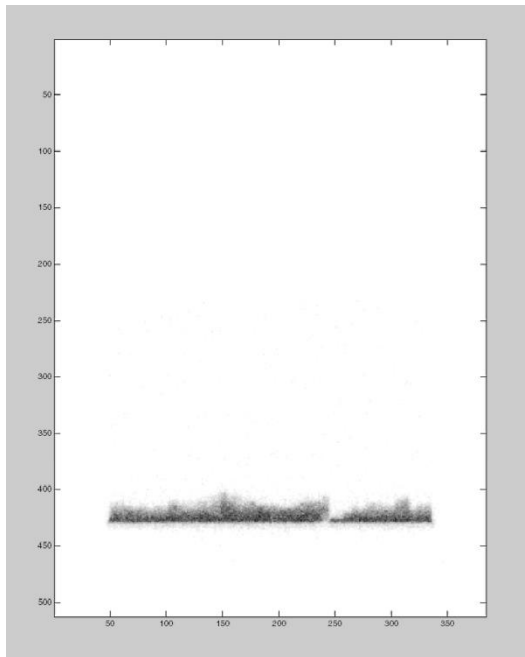
4D exit phase space in DOSXYZnrc coordinates

‘Exit detector’ 4D phase space

DOSXYZnrc  
isource=20  
simulation



MC  
simulation  
of  
cumulative  
EPID dose



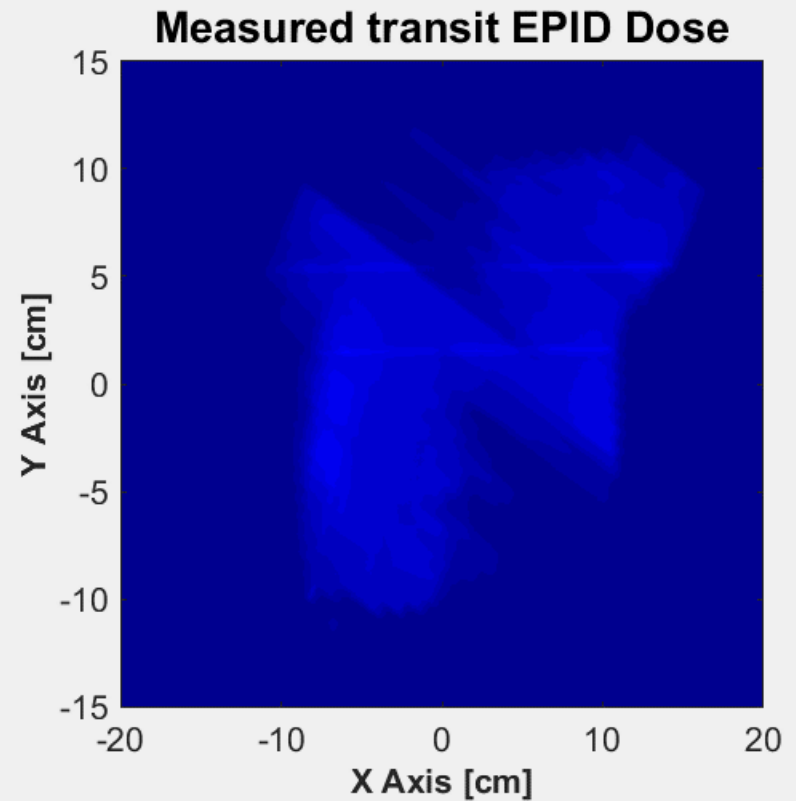
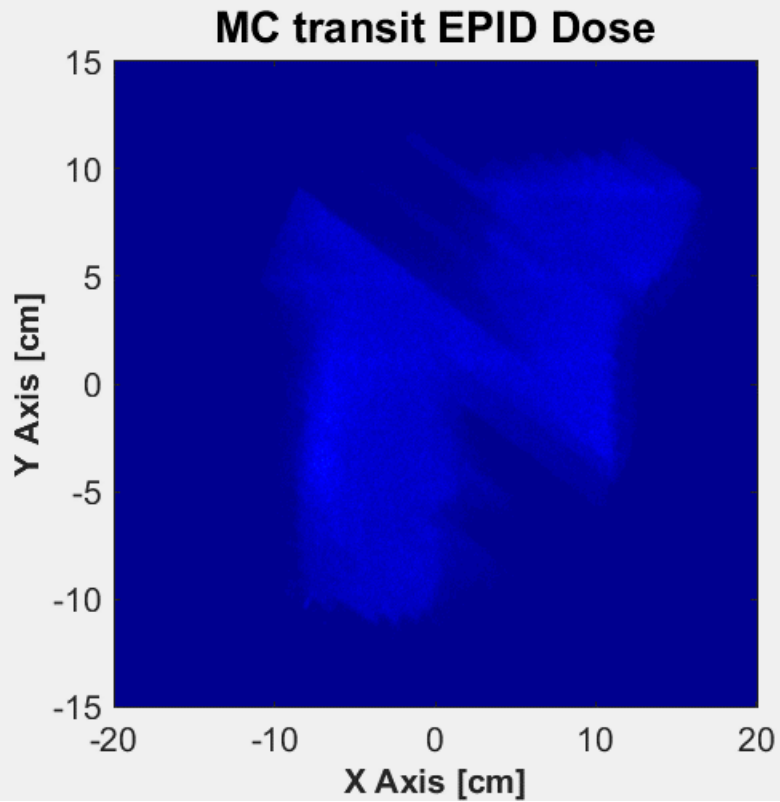
Actual  
cumulative  
EPID  
image,  
acquired in  
CineMode



# Advantages of “time-stamping” particles:

- Efficiency
  - Only one simulation required
  - Similar simulation time as conventional MC
- 4D dose data: [filename].edepdat
  - Contains all required dose information
  - No need for pre-defined interval of interest

# Results ---- MC vs. Measurement



# Results ---- MC vs. Measurement

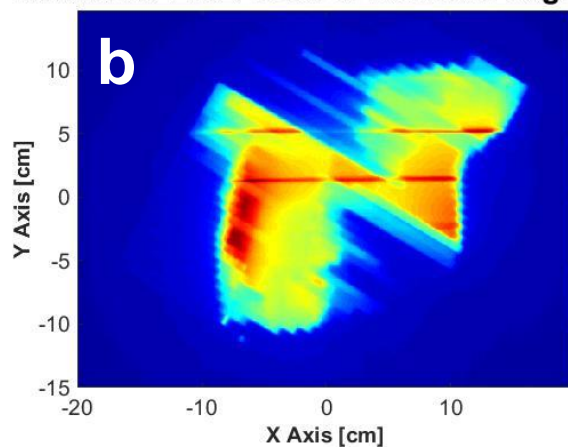
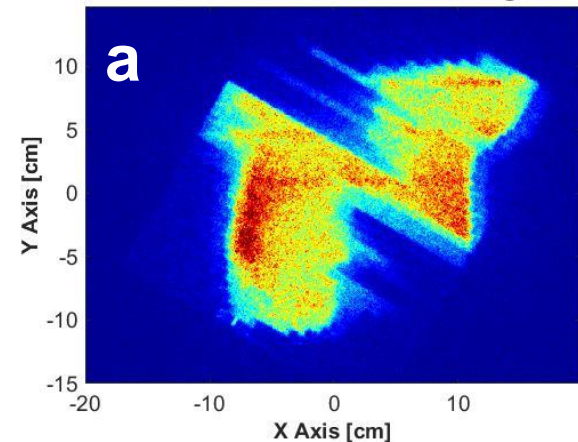
## Dose for a single control point

MC EPID Dose of Random Segment

Measured EPID Dose of Random Segment

3D Gamma  
pass rates:

98.5%

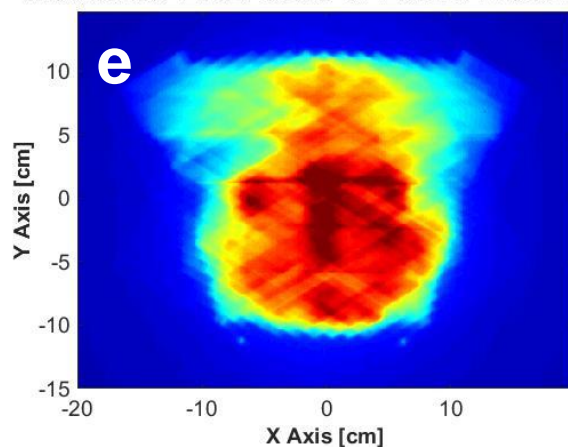
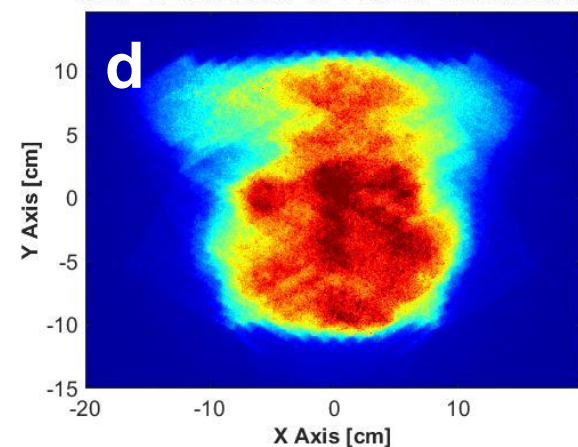


## Cumulative dose

MC EPID Dose of Entire Treatment

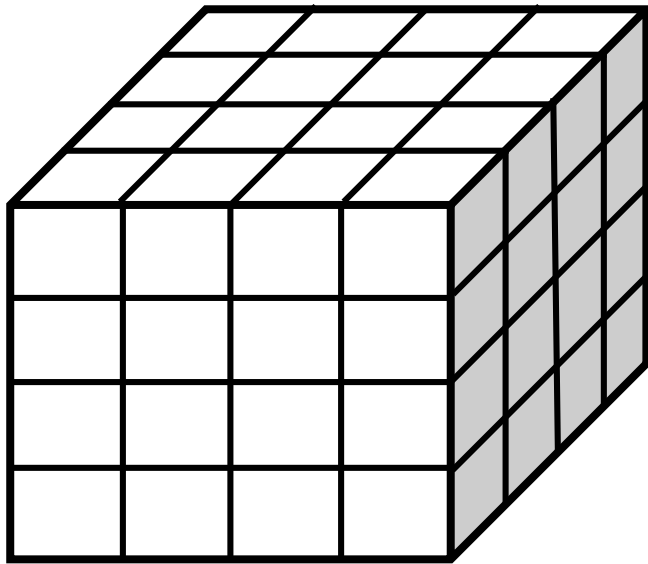
Measured EPID Dose of Entire Treatment

96.0%

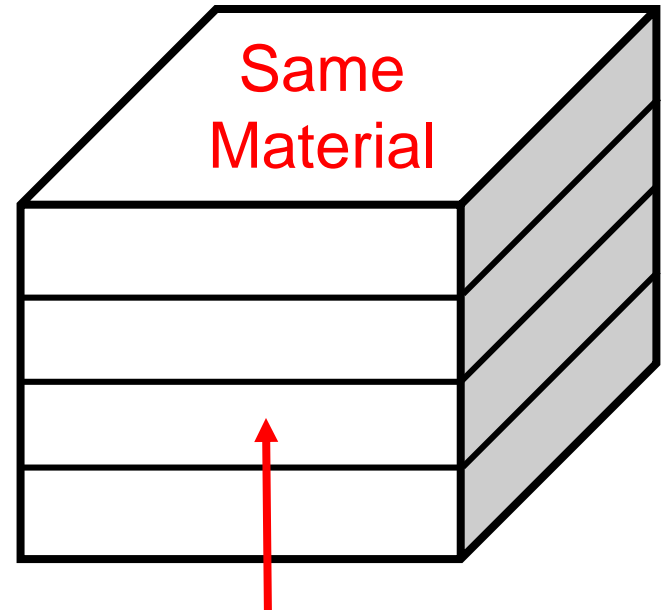


# Faster simulation using slab phantom

512 × 384 × 20 voxels



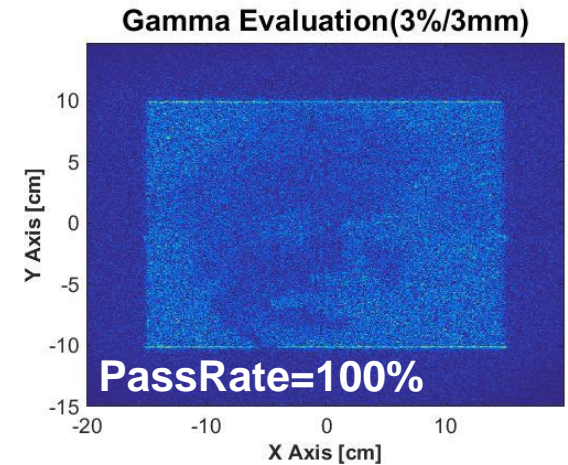
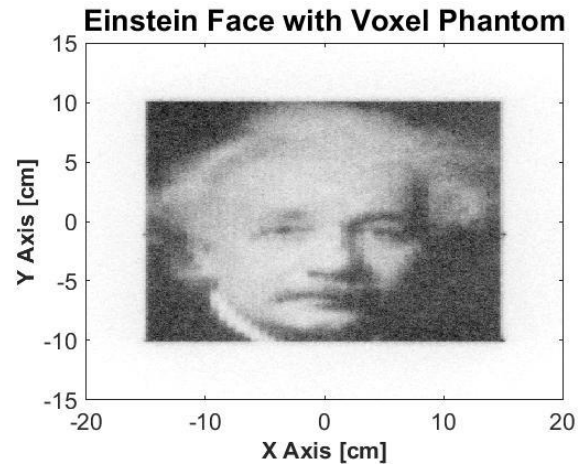
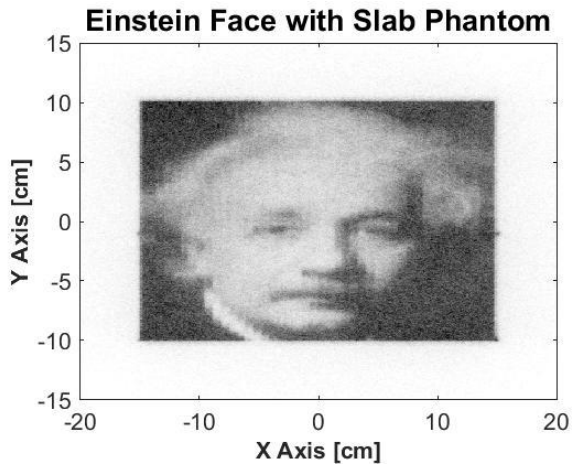
20 slabs



- Record 3D coordinates of energy deposition events
- Voxelization after simulation

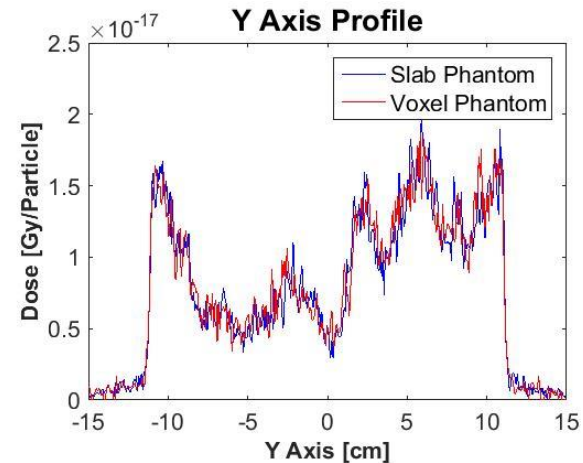
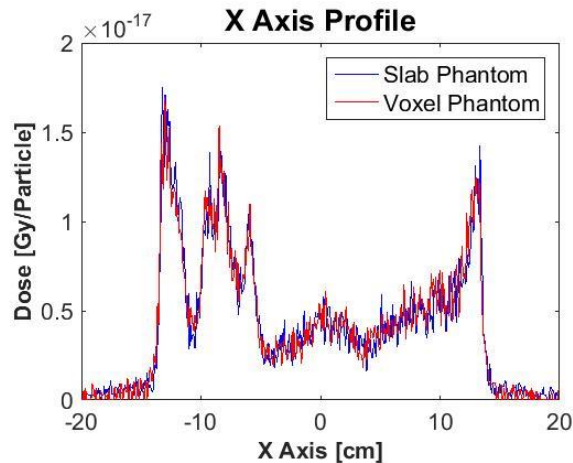


# Slab Phantom vs. Voxel Phantom



3

30  
mins



```
1 EPID_VMAT_prostate_phsp_out #!GUI1.0
2 0
3 /home/tpopescu/EGS_HOME/dosxyznrc/Varian_iX_EPID_slab.egsphant
4 0.521, 0.01, 0
5 0, 0, 0,
6 2, 20, 2, 0, 0, 0, 0, 0, 0
7 0, -47.64, 0, 90, 270.0, 240, 100.0, 0.0
8 0, -47.64, 0, 90, 270.0, 240, 100.0, 1.0
9 2, 2, 0, 120, 0, 0, 0, 0
10 0, /home/tpopescu/EGS_HOME/dosxyznrc/VMAT_prostate_out.IAEAphsp,0
11 500000000000, 0, 999, 87, 911, 100.0, 0, 0, 3, 1, 1, 0, 0, 0, 1, 0
12 #####
13 :Start MC Transport Parameter:
14
15 Global ECUT= 0.521
16 Global PCUT= 0.01
17 Global SMAX= 5
18 ESTEPE= 0.25
19 XIMAX= 0.5
20 Boundary crossing algorithm= PRESTA-I
21 Skin depth for BCA= 0
22 Electron-step algorithm= PRESTA-II
23 Spin effects= 0n
24 Brems angular sampling= Simple
25 Brems cross sections= BH
26 Bound Compton scattering= Off
27 Compton cross sections= default
28 Pair angular sampling= Simple
29 Pair cross sections= BH
30 Photoelectron angular sampling= Off
31 Rayleigh scattering= Off
32 Atomic relaxations= Off
33 Electron impact ionization= Off
34 Photon cross sections= xcom
35 Photon cross-sections output= Off
36
37 :Stop MC Transport Parameter:
38 #####
```

Images for a VMAT prostate patient, acquired during treatment (left) and MC simulated with  $1.5 \times 10^9$  histories (right):

Cumulative images

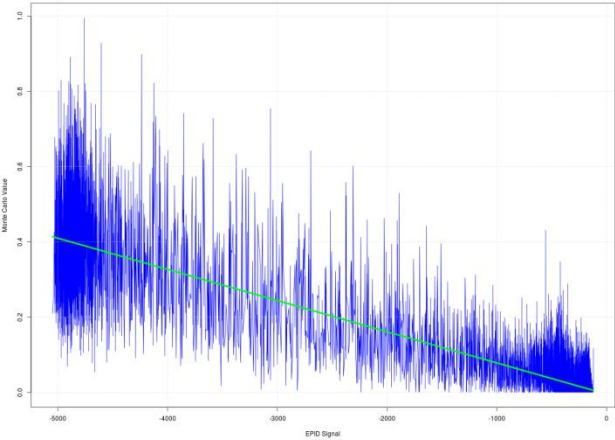


Images for a VMAT prostate patient, acquired during treatment (left) and MC simulated with  $1.5 \times 10^9$  histories (right):

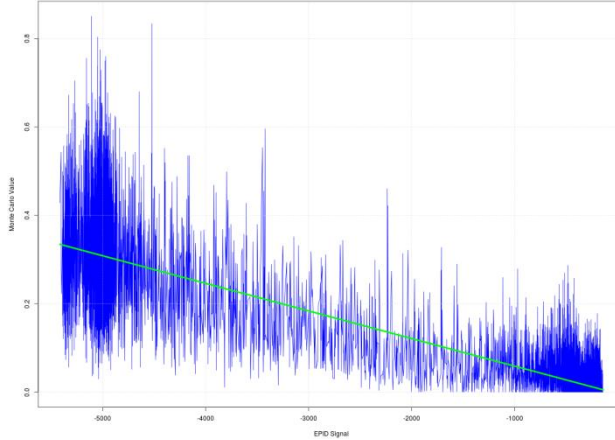
Cine-mode images



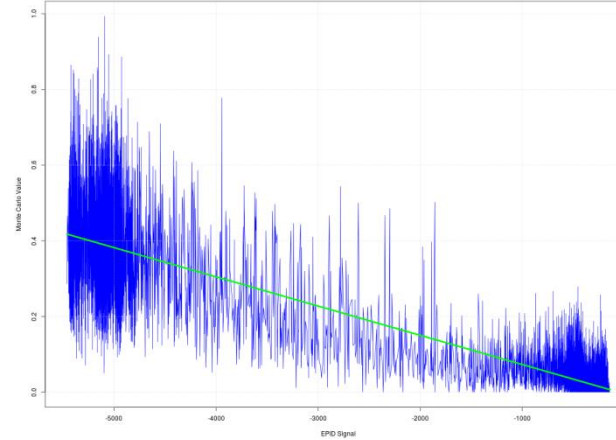
MC = (-4.2910087877521e-05) \* EPID + (-0.0047970529364001)



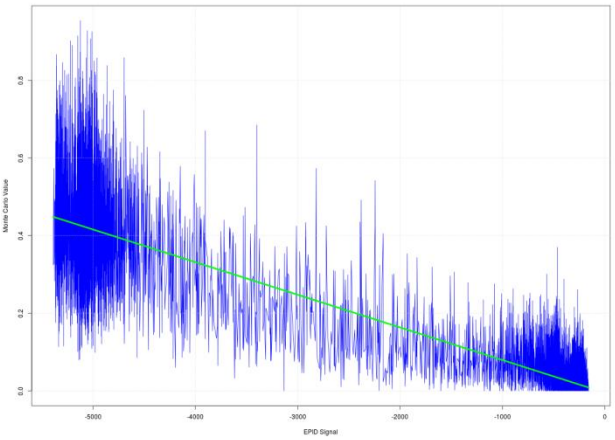
MC = (-4.2382443374018e-05) \* EPID + (-0.0034521753283517)



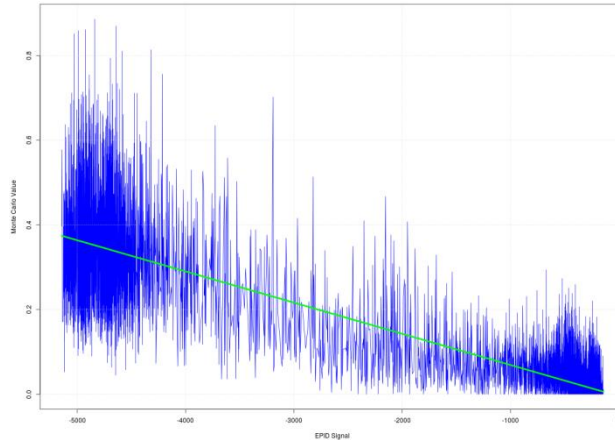
MC = (-7.72399533462015e-05) \* EPID + (-0.00428593760718081)



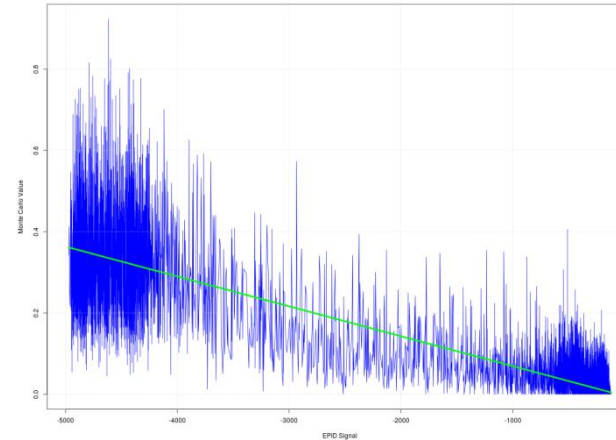
MC = (-4.4054726163048e-05) \* EPID + (-0.0045736896620493)



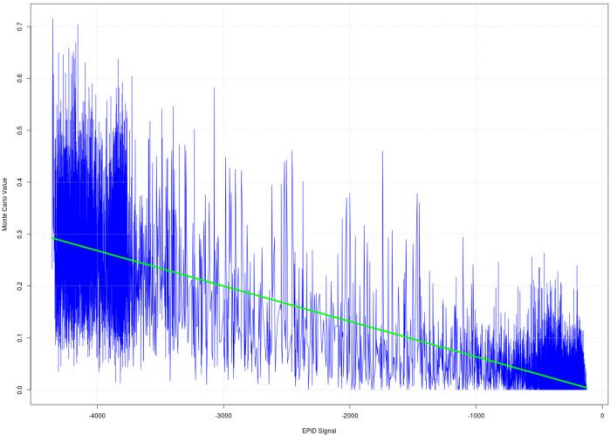
MC = (-7.3644091503779e-05) \* EPID + (-0.0045601380410491)



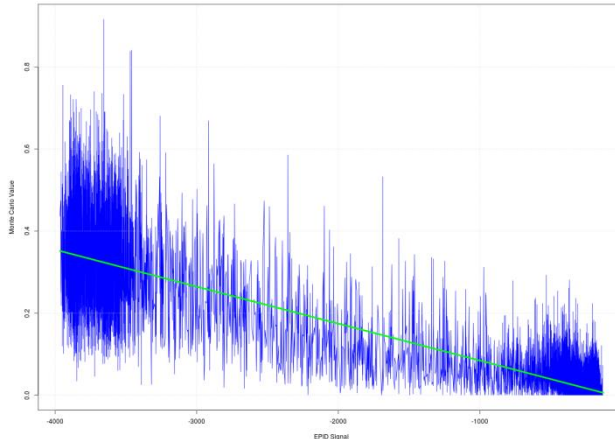
MC = (-7.35167541445301e-05) \* EPID + (-0.00426583478399796)



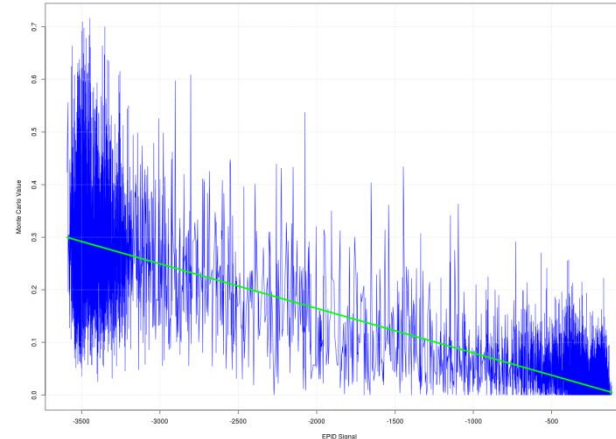
MC = (-4.81094813599433e-05) \* EPID + (-0.00441424806042235)



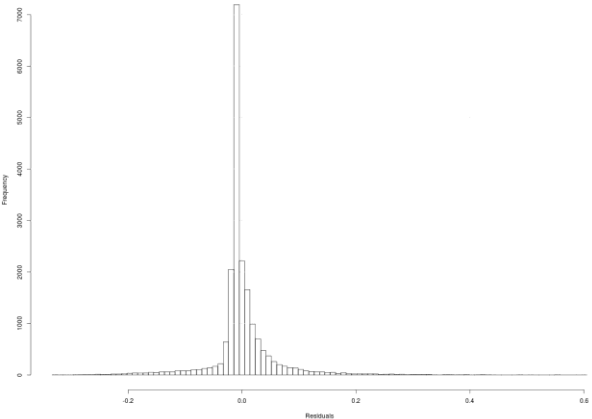
MC = (-9.0120206088372e-05) \* EPID + (-0.00583502842199379)



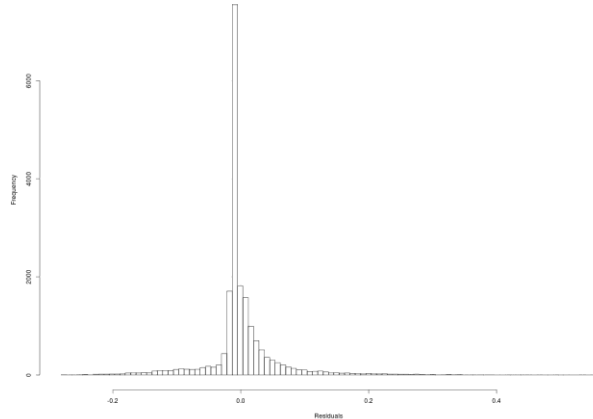
MC = (-4.47934052573795e-05) \* EPID + (-0.00486446791028039)



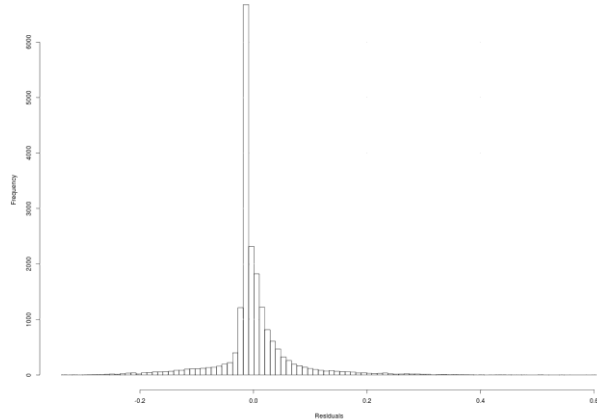
Standard Deviation = 0.055855229699508



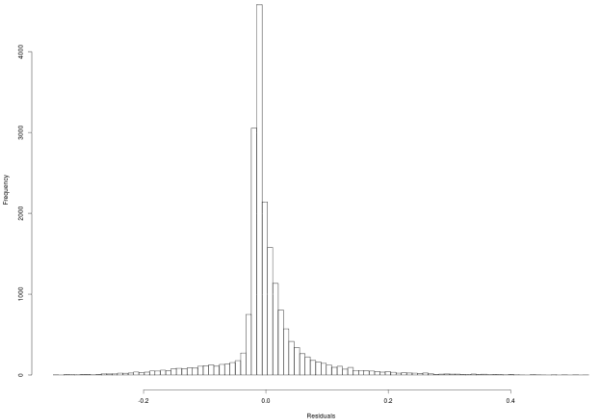
Standard Deviation = 0.054304872434187



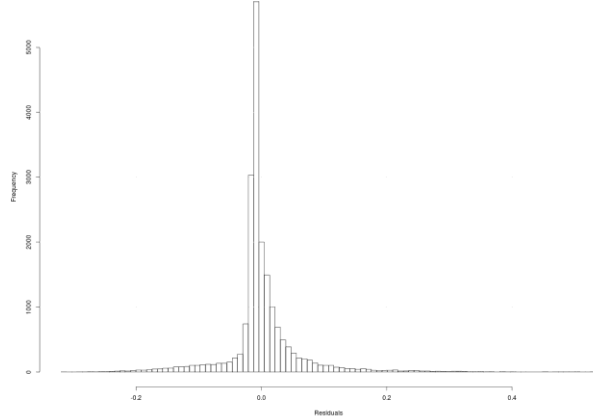
Standard Deviation = 0.062005062627709



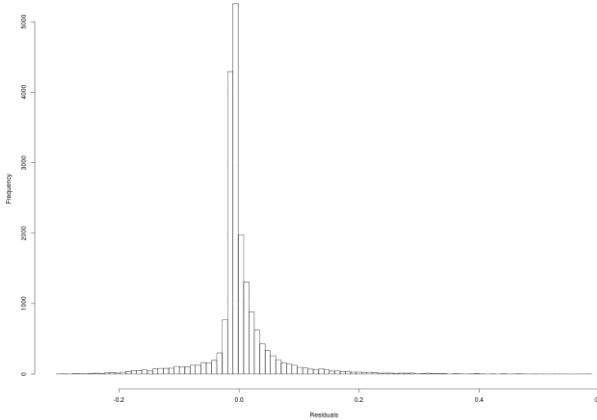
Standard Deviation = 0.0653421822752957



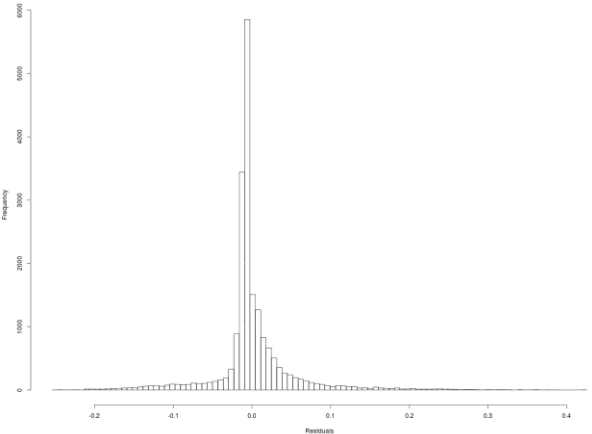
Standard Deviation = 0.056580982060488



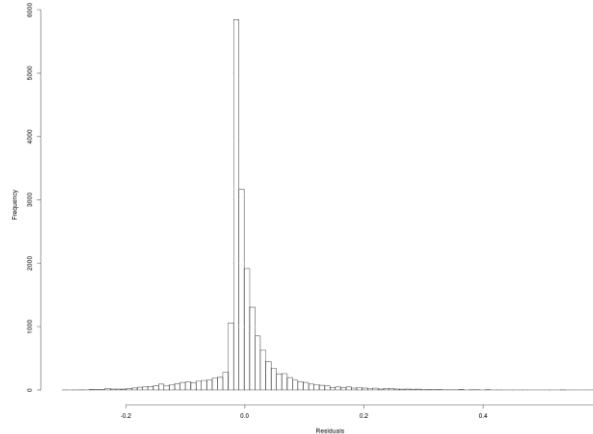
Standard Deviation = 0.0556474702278285



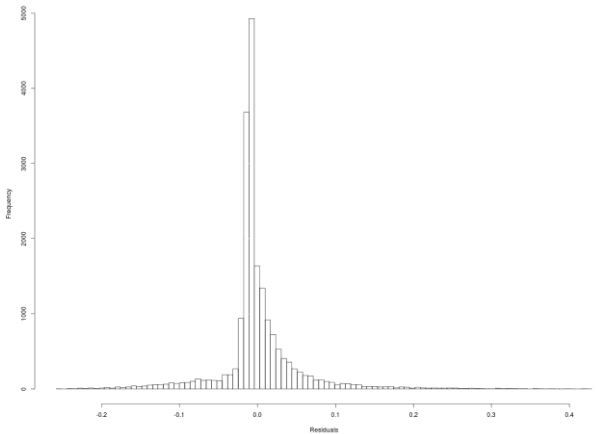
Standard Deviation = 0.0503207229351051



Standard Deviation = 0.056687685901494



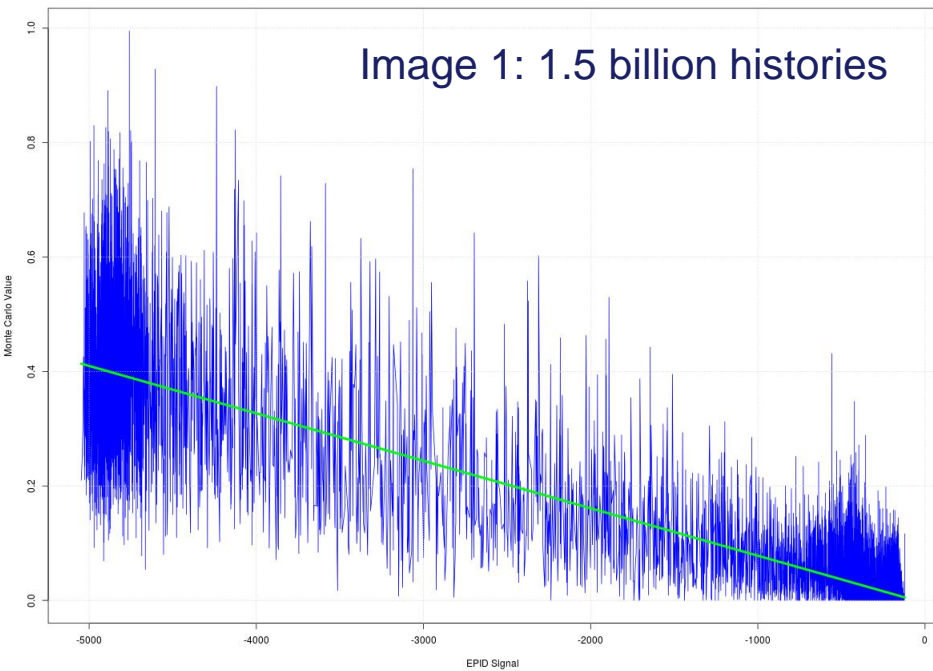
Standard Deviation = 0.051486362975207



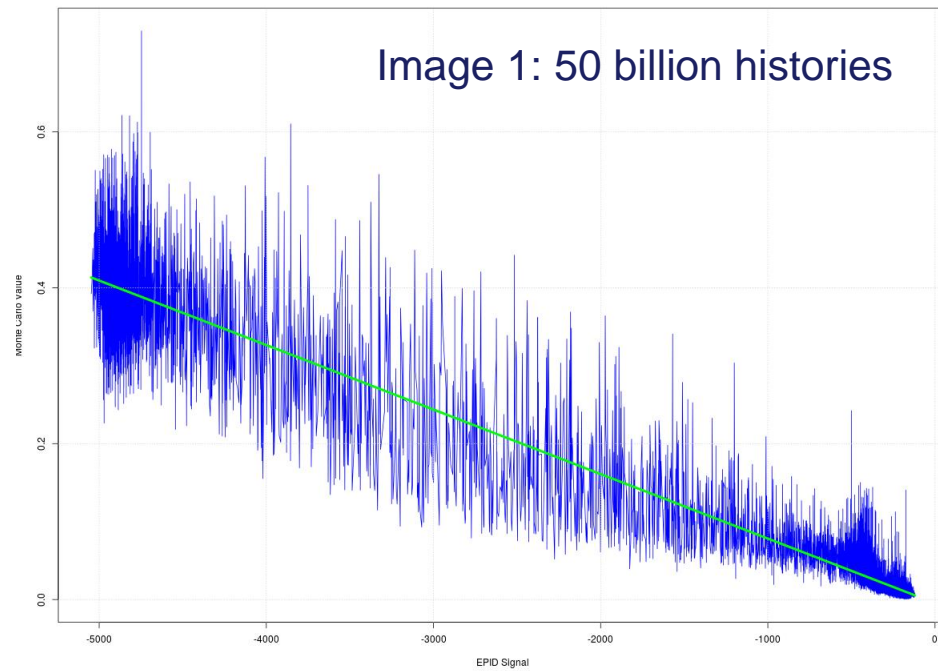
## Linear fit and statistics of the residuals

<b>EPID File Name</b>	<b>MC File Name</b>	<b>Correlation Coefficient</b>	<b>Slope</b>	<b>Intercept</b>	<b>Min Residuals</b>	<b>Max Residuals</b>	<b>StDev of Residuals</b>
epid_01.Rdata	mc_01.Rdata	-0.90587	-0.000082910	-0.004797	-0.333545	0.605131	0.0559
epid_02.Rdata	mc_02.Rdata	-0.89565	-0.000062382	-0.003452	-0.281118	0.555170	0.0543
epid_03.Rdata	mc_03.Rdata	-0.91569	-0.000077240	-0.004286	-0.338864	0.604519	0.0620
epid_04.Rdata	mc_04.Rdata	-0.91957	-0.000084055	-0.004574	-0.347858	0.527754	0.0653
epid_05.Rdata	mc_05.Rdata	-0.90643	-0.000073644	-0.004560	-0.319605	0.534049	0.0566
epid_06.Rdata	mc_06.Rdata	-0.90372	-0.000073517	-0.004266	-0.304656	0.587691	0.0556
epid_07.Rdata	mc_07.Rdata	-0.88405	-0.000068109	-0.004414	-0.254017	0.425657	0.0503
epid_08.Rdata	mc_08.Rdata	-0.89793	-0.000090120	-0.005835	-0.306793	0.592821	0.0567
epid_09.Rdata	mc_09.Rdata	-0.89324	-0.000084793	-0.004864	-0.258157	0.428704	0.0515

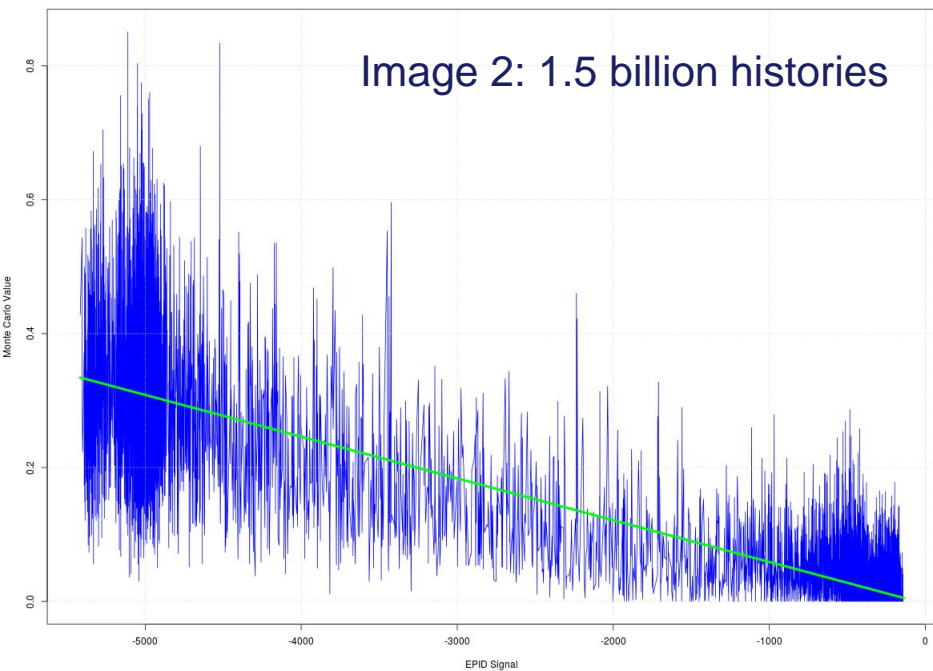
MC = (-8.29100878777521e-05) \* EPID + (-0.00479703629364001)



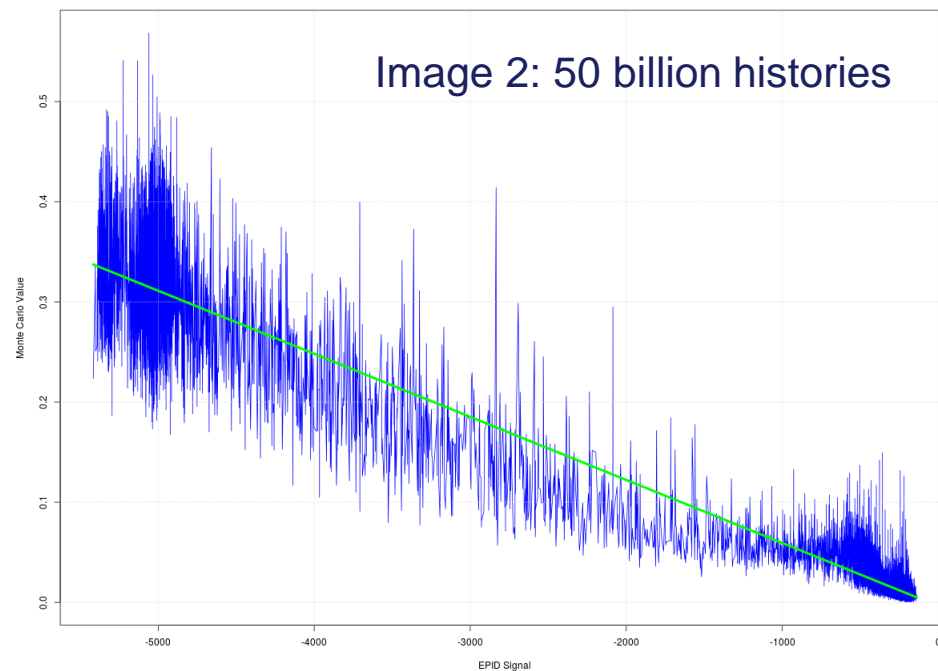
MC = (-8.27542418968348e-05) \* EPID + (-0.00457416966183619)



MC = (-6.238244374018e-05) \* EPID + (-0.00345217532833517)

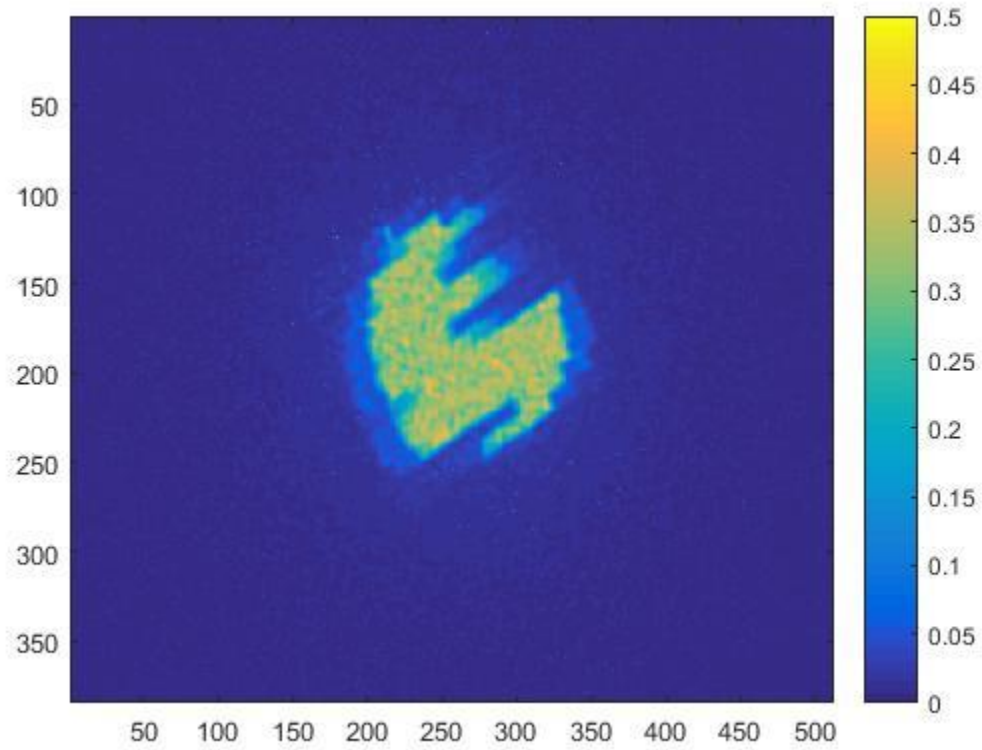


MC = (-6.29485983379689e-05) \* EPID + (-0.00364636935573657)

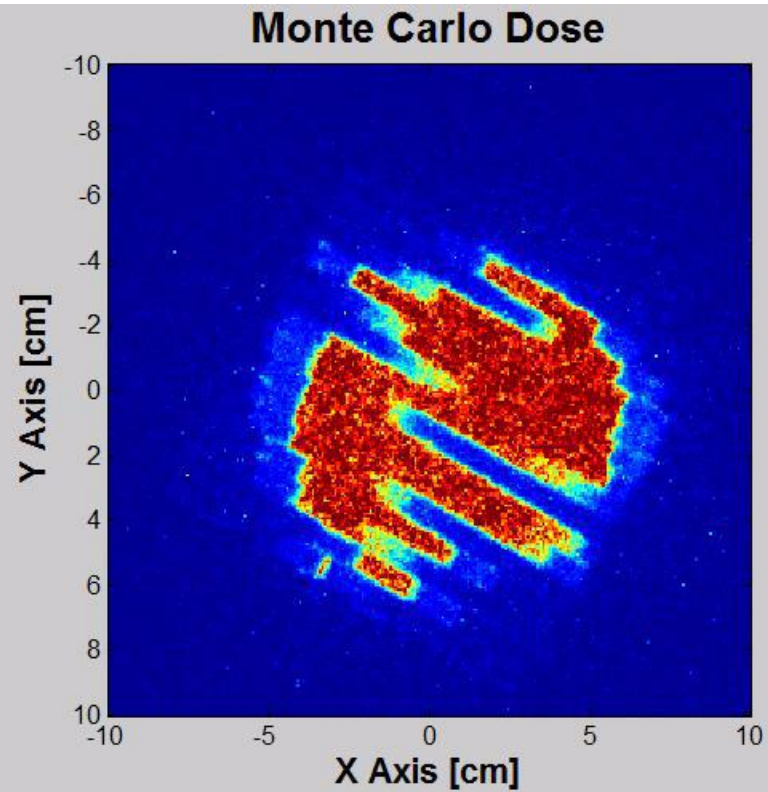
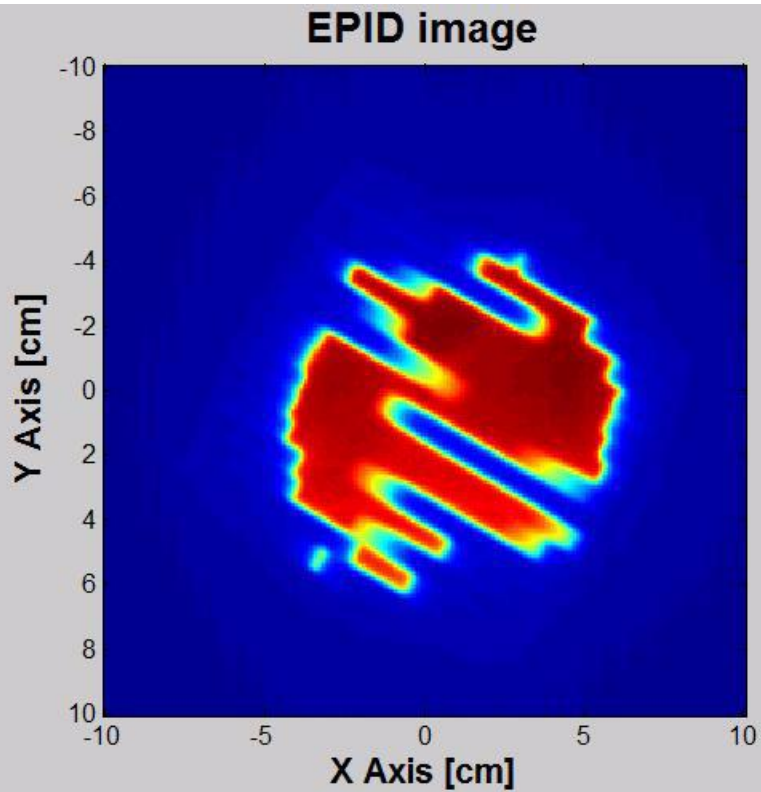




After applying a Savitzky-Golay denoising filter:

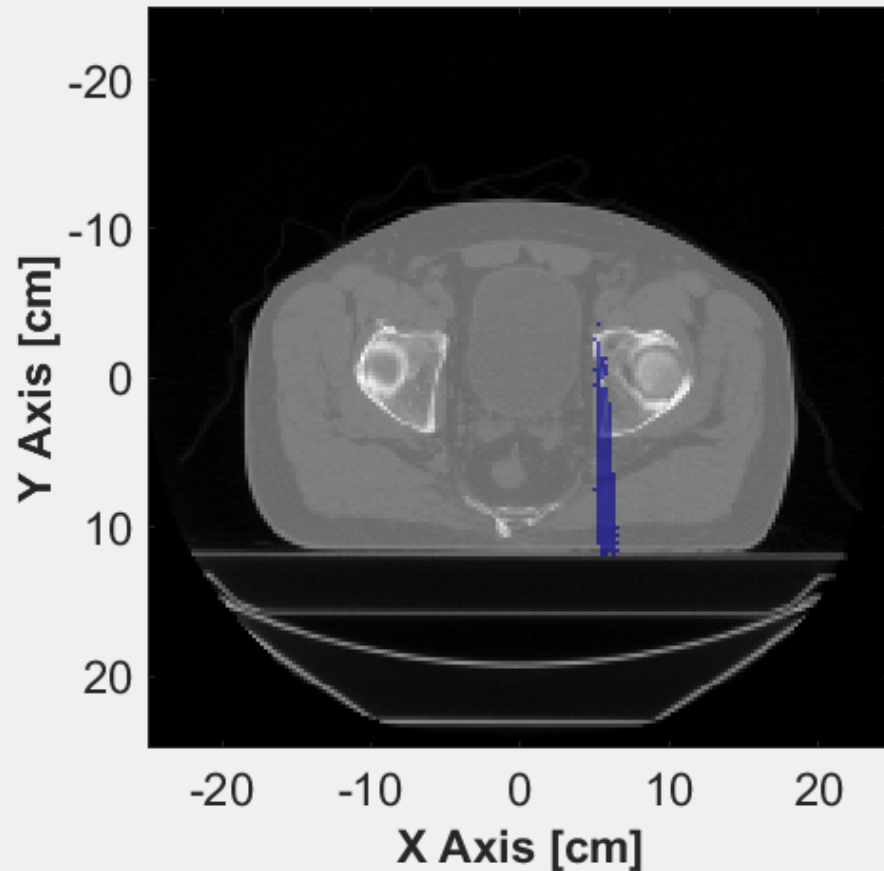


Images for the same patient, simulated with  $5 \times 10^{10}$  histories:



# 4D MC simulation with BEAMnrc/DOSXYZnrc

**Dose accumulation of prostate case**



# A simple and robust trajectory-based stereotactic radiosurgery treatment

Byron Wilson<sup>a)</sup>

*Physics and Astronomy, University of British Columbia, Vancouver, British Columbia V6T 1Z4, Canada  
Medical Physics, BC Cancer Agency, Vancouver, British Columbia V5Z 4E6, Canada*

Karl Otto

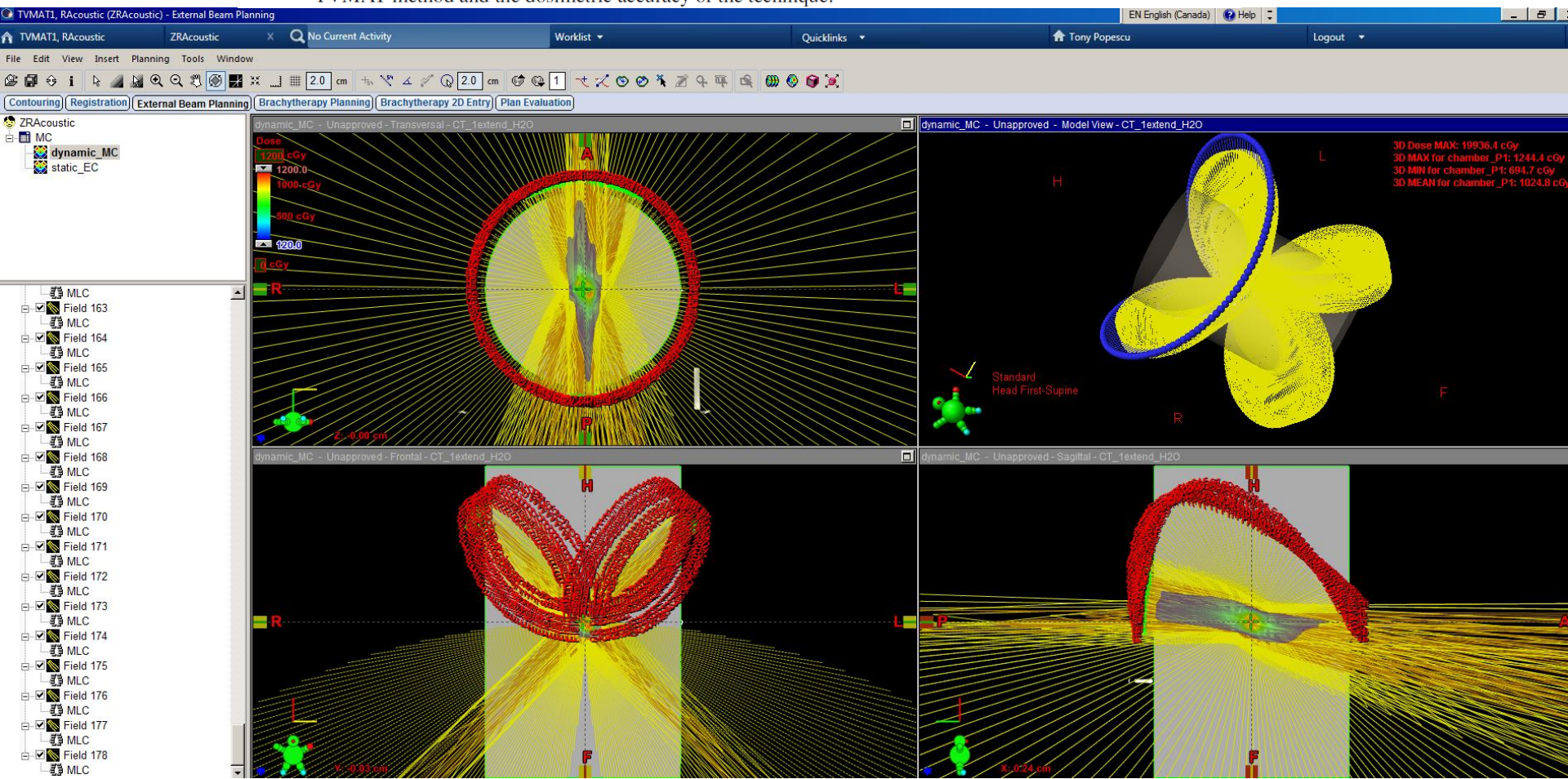
*Physics and Astronomy, University of British Columbia, Vancouver, British Columbia V6T 1Z4, Canada*

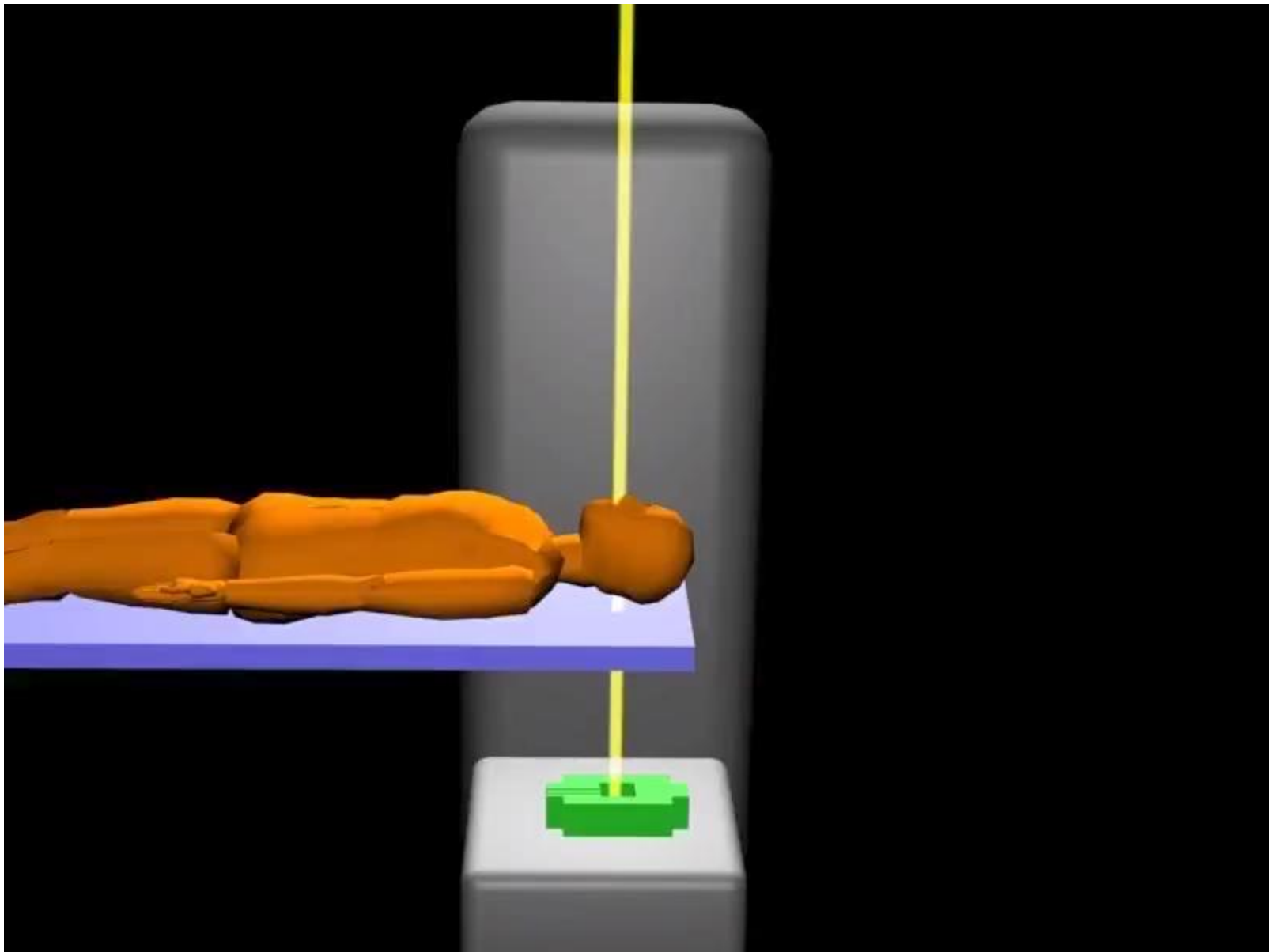
Ermias Gete

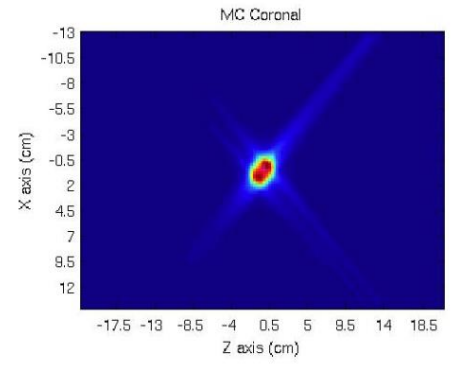
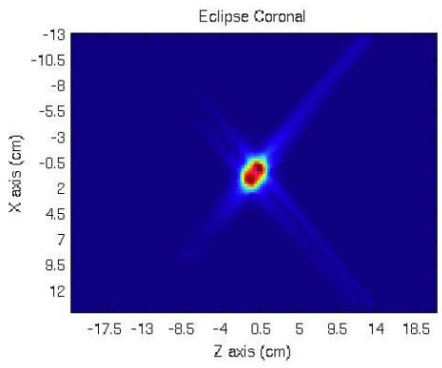
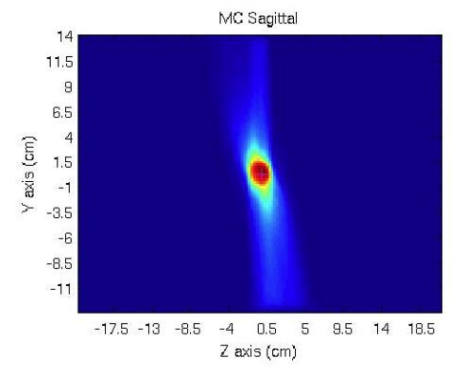
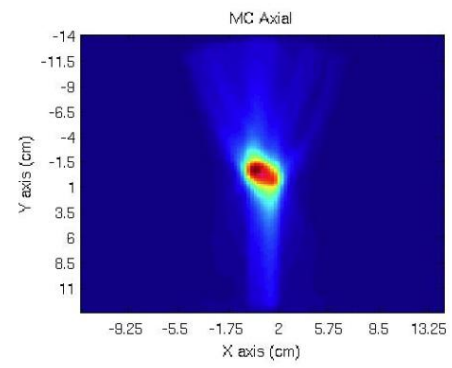
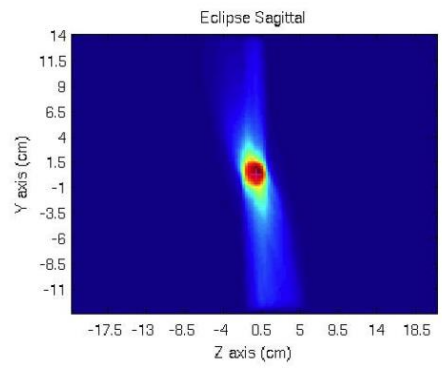
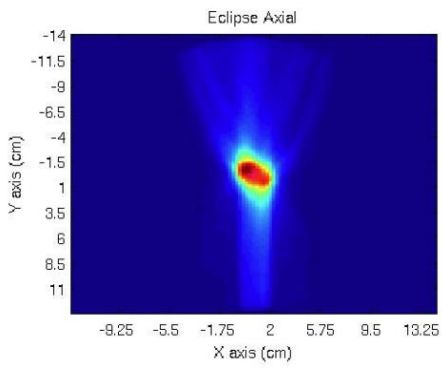
*Medical Physics, BC Cancer Agency, Vancouver, British Columbia V5Z 4E6, Canada*

(Received 7 June 2016; revised 20 September 2016; accepted for publication 21 November 2016; published 19 January 2017)

**Introduction:** We present a Trajectory-based Volumetric Modulated Arc Therapy (TVMAT) technique for Stereotactic Radiosurgery (SRS) that takes advantage of a modern linacs ability to modulate dose rate and move the couch dynamically. In addition, we investigate the quality of the developed TVMAT method and the dosimetric accuracy of the technique.







First few control points in the DOSXYXnrc Source 20 egsinp file:

```

0.000, -28.300, -87.887, 90, 91.00, 240, 100.0, 0.0000
0.000, -28.300, -87.887, 88, 90.04, 151, 100.0, 0.0056
0.000, -28.300, -87.887, 86, 90.14, 152, 100.0, 0.0113
0.000, -28.300, -87.887, 84, 90.32, 153, 100.0, 0.0169
0.000, -28.300, -87.887, 82, 90.58, 154, 100.0, 0.0226
0.000, -28.300, -87.887, 80, 90.91, 155, 100.0, 0.0282
0.000, -28.300, -87.887, 78, 91.31, 156, 100.0, 0.0339
0.000, -28.300, -87.887, 76, 91.80, 157, 100.0, 0.0395
0.000, -28.300, -87.887, 74, 92.36, 158, 100.0, 0.0452
0.000, -28.300, -87.887, 72, 93.01, 160, 100.0, 0.0508
0.000, -28.300, -87.887, 70, 93.74, 161, 100.0, 0.0565
0.000, -28.300, -87.887, 68, 94.56, 162, 100.0, 0.0621
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0.000, -28.300, -87.887, 64, 96.48, 165, 100.0, 0.0734
0.000, -28.300, -87.887, 62, 97.59, 166, 100.0, 0.0791
0.000, -28.300, -87.887, 61, 98.80, 168, 100.0, 0.0847

```

3D Gamma: 97.1%

## Conclusions:

- We developed a fast, all-in-one, DOSXYZnrc simulation technique for cine-mode EPID images, for the purpose of comparisons with the actual images acquired while the patient is being treated.
  
- In addition, the patient dose could be simulated and accumulated over the entire course of treatment (ideally, in an adaptive manner, using daily CBCT data), resulting in an authentic 'patient-specific QA'.

## Acknowledgements:

### *International collaborators:*

**Blake Walters**

**Frederic Tessier**

**Frank Verhaegen**

**Dave Rogers**

**Iwan Kawrakow**

**Emily Heath**

**Cecilia Borges**

**Jan Seuntjens**

**Jeff Siebers**

**Rickard Cronholm**

**James Robar**

**Alan Nahum**

**Jarkko Ojala**

### *Local collaborators:*

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**Shiqin Su**

**Iulian Badragan**

**Parmveer Atwal**

**Alanah Bergman**

**Tony Teke**

**John Lucido**

**Ernest Tsang**

**Vitali Moiseenko**

**Byron Wilson**

**Ermias Gete**

**Karl Otto**

### *Research funding:*

**British Columbia Cancer Agency**

**Varian Medical Systems**



# Thank you !



Photo of Mt. Baker (an active volcano), as seen from Vancouver Island